Design Development and Characterisation of Tramadol Hydrochloride Loaded Transethosomal Gel Formulation for Effective Pain Management

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ABSTRACT

Introduction: The purpose of the present study was to design develop and characterize the tramadol hydrochloride loaded transethosomal gel formulation for effective pain management. Materials and Methods: The transethosomes were prepared by simple cold method. Total 12 formulations were prepared using different concentrations of phospholipid (Soya lecithin and L-α Phosphatidylcholine from egg yolk) and edge activator (Span 20 and Cremophor EL 35). The developed transethosomes were characterized for FTIR, drug content, EE, particle size, zeta potential, TEM, in vitro drug release and release kinetics. The optimised formulation was selected for preparation of transethosomal gel. The formulated gel was estimated for viscosity, drug content, EE and stability study for 28 days. Results and Discussion: The zeta potential of best formulation was -22mV, the particle size was at the range of 149.34 nm to 278 nm. Span 20 formulations exhibit a faster drug release (91.91 to 95.7%) than the Cremophor formulations, whose release exhibits an extended pattern (78.96% to 79.34%) at the end of 8th hr. Optimised formulation follows first order kinetics and its R2 value is 0.991. Conclusion: The study supports the development of optimised transethosome formulation into a topical gel using carbopol 934 as gelling agent. The viscosity of the gel formulation was 30168 cps. The drug content and EE was found to be 91.52% and 79.37% respectively. Stability studies prove that there is very less change in the EE, hence the formulation was found to be stable.

Key words: Tranethosomes, Tramadol hydrochloride, Phospholipid, Edge activator, Entrapment efficiency.

INTRODUCTION

Topical drug delivery of active pharmaceutical carriers, which a drug is delivered in the targeted area under controlled system can have a significant effect on efficacy. The main advantage of the topical drug delivery is to bypass first pass metabolism. Topical drug carriers are used for the localized effect of application and deliver the drug into underlying percutaneous layers of the skin. These systems can be characterized as controlled and targeted drug delivery systems. The systems raise the efficacy of the drug and dominate the side effects for the improved patient compliance. The polar drug molecules are encapsulated into the hydrophobic channel carrier which is prevented from hydrolysis and enzymatic degradation. The ethosomal carriers are vesicular systems that comprise phospholipids, water and a moderately increased concentration of ethanol. Ethosomal systems are of three type’s namely classical ethosomes, binary ethosomes and transethosomes (TEs). These are of novel generation and developed in 2012. They usually comprises of ethosomes and an edge activator or a penetration enhancer. The transethosomes improves the physical and chemical qualities of the therapeutic drug enclosed in dermal...
and transdermal delivery. The effect of enhancement is proven by several researchers.6-8 These transethosomes contain high concentration of ethanol which induces hydration of the outer layer of the skin and widen the pores and initiate the drug release to the targeted site. The transethosomes are prepared by using cold method.9,10 The cold method is simple and widely used method for the preparation of transethosomes. Tramadol hydrochloride is a centrally acting analgesic which is used to treat mild pain to severe pain. The drug is recommended for nociceptive pain commonly responsive to anti-inflammatory agents and opiates. Tramadol hydrochloride shows high solubility and permeability which increase its concentration in the central nervous system. Tramadol hydrochloride loaded transethosomal topical gel formulation reduces the adverse effects of the drug and increases the therapeutic efficacy. Transethosomes penetrate and target the stimulation of specialized nerve endings pain receptors which sense and respond to the damaged nerves. Phospholipids from different sources have been used in the transethosomal system, the type of phospholipid used influences the vesicle formation of the transethosomes.11,12 The L-α-phosphatidylcholine from egg yolk lyophilized powder and soya lecithin is used as encapsulating agent in the preparation of transethosomes.13 The type of edge activator used has a significant role in the size, stability and used to increase the penetration of active drug into the skin. The selection of the edge activator is the critical step in formulation of the transethosomes. Span 20 and Cremophor EL-35 were used as edge activators. The incorporation of edge activators prevents the leakage of the vesicles and maintains the vesicular charge. Ethanol is the solvent system used as the penetration enhancer which helps in fluidization of the skin stratum corneum and helps the release of the drug to the underlying layers of the skin. These transethosomal systems were incorporated into suitable gelling systems which are compatible and provide required viscosity and bio adhesive properties.14 Incorporating into the gelling agent results in controlled release of the drug and prevent the loss of the drug from the transethosomal vesicles. This advance method of formulation of transethosomes helps to cutdown the side effects of the orally consumed drugs for minor pains and topically deliver the drug to effected targeted area in a controlled system. The focus of the present study is to develop and characterize transethosomal gel carriers for topical delivery of tramadol hydrochloride as a route for the drug administration. In this study tramadol hydrochloride encumbered TEIs were prepared with various concentrations of solvent system and edge activator. The optimised formulation was incorporated into a gel base.

**MATERIALS AND METHODS**

Tramadol hydrochloride was collected gifted sample from Aurobindo Pharma Pvt Ltd, Hyderabad. Span 20, Cremophor EL-35 was obtained from Lobachem. Soya lecithin and L-α-phosphatidylcholine from egg yolk lyophilized were purchased from Sigma - Aldrich, Mumbai. Carbopol 934 was obtained from CDH, New Delhi. The chemicals utilized in the research are of AR grade were procured from Merck, Mumbai.

**Preparation of tramadol hydrochloride loaded TEs**

The cold method was used for the preparation of tramadol hydrochloride transethosomes. A solution of phosphatidylcholine and surfactant (Span20, Cremophor EL-35) in ethanol at 30°C act as organic phase. The aqueous phase / ultra pure water was heated at 30°C and then delivered to the organic phase drop wise with constant mixing at 700 rpm with the help of magnetic stirrer. Continue the stir for 45 min to bring the transethosomal dispersions that were supplemented for size-reduction by probe sonication for 10 mins at room temperature. The method was found to give more stable transehthosomes. The composition of these formulations was shown in Table 1.

**Evaluation of Transehthosomes**

**Drug Excipient compatibility study**

The drug interaction and the composition compatibility within the formulation ingredients were determined using FT-IR analysis. The IR spectrum was performed by using a (Bruker FTIR) spectrophotometer. The samples were recorded using the conventional KBr pellet method. The samples were scanned in the region between 4000 and 400cm⁻¹ with a resolution of about 4cm⁻¹.

**Assay**

The drug content in the developed transehthosome formulation was determined. An amount of transethosomes containing tramadol hydrochloride equivalent to 100mg were weighed and suspended in suitable media. This was conserved for about 20 min for thorough mixing. Agitate continuously and filter by 0.45µm membrane filter. The amount of tramadol present was estimated at 271nm using a regression equation through the linearity plot.15

**Drug content = Sample absorbance / Standard absorbance × 100**
Percentage drug EE
The EE was estimated using mini column centrifugation method. The samples were wrecked to centrifugation at 8000 rpm. The supernatant was discarded the obtained sediment was dissolved in mixture of dichloromethane and methanol. The sediment was suspended in suitable media and the absorbance was taken at 271nm.\textsuperscript{16,17} The drug EE was quantified by applying the below equation
\[
EE\% = \frac{\text{Amount of entrapped drug}}{\text{Total amount of drug}} \times 100
\]

Evaluation of vesicle size
Vesicle size was assessed by DLS (dynamic light scattering) using a programmed scrutiny system and Photon Correlation Spectroscopy (PCS). The size of transethosomes ranges between nanometres and is influenced by the composition of the formulation. Size and size distribution of transethosomes were carried out using Beckman coulter particle size analyser (Delsa™ Nano Common). The transethosome was distributed in double distilled water prior to administration of the sample in the instrument, to establish that the signal of light scattering, as indicated by particle count/second was in the instrument’s sensitivity range.\textsuperscript{18}

Transethosomes Morphology
Shape and morphology of the TEs was investigated using transmission electron microscopy. An aqueous solution of 2% w/v phosphotungstic acid on a copper grid (carbon-coated) was used to stain negatively the prepared transethosomes and was examined by TEM (FEI Tecnai G2 F20 S-twin/EDAX). The prepared transethosome was dropped onto the carbon coated grid; the additional solution was extracted using a blotting paper. Allow the grid to dry for 5 min.\textsuperscript{18} The TEM micrograph was taken by applying an accelerating voltage of 200 kV.

Zeta potential
The surface charge of TEs was estimated by conducting Zeta potential measurements. The estimation was conducted in distilled water with conductivity regulated to 0.0504 ms/cm. Zeta potential was checked in the original dispersion medium (water).\textsuperscript{19} The analysis was performed using the Beckman Coulter (Delsa™ Nano Common).

In vitro drug release
The release studies were estimated by Franz diffusion cell. A cellophane dialysis membrane (Hi-media 60) was hydrated with phosphate buffer (pH 7.4). Two millilitres of the TEs equivalent to 100 mg of tramadol hydrochloride was kept in donor compartment.\textsuperscript{17} The receptor compartment was replete with pH 7.4 and mixed with a magnetic bar at 500 rpm at 37±1°C. The required sample was taken off at predetermined time intervals for 8 h and was assessed for tramadol hydrochloride content by UV spectrophotometrically at 271 nm.

Analysis of release mechanism
The release mechanisms and the design of therapeutic device mathematical models are widely employed. The study of in vitro release profile of formulations was done by implementing appropriate release data in several drug release models including zero order, first order and Higuchi. The mentioned models are well known for the characterization drug dissolution / release profile.

Preparation of tramadol hydrochloride loaded TEs gel
Tramadol hydrochloride-loaded TEs gel was prepared by including the requisite quantity of the optimized tramadol hydrochloride enclosed TEs in a previously

| Table 1: Composition of Tramadol Hydrochloride Transethosome Formulation F1- F12. |
|-------------------|---|---|---|---|---|---|---|---|---|---|---|---|
| Ingredients       | F 1 | F2 | F 3 | F 4 | F 5 | F 6 | F7 | F8 | F 9 | F10 | F11| F 12 |
| Tramadol (mg)     | 100 | 100| 100| 100| 100| 100| 100| 100| 100| 100| 100| 100 |
| Soya lecithin (SC)| 2 % | 3% | 5% | -  | -  | -  | 2% | 3% | 5% | -  | -  | -  |
| L-α Phosphatidylcholine from egg yolk (PL)| -  | -  | -  | 2% | 3% | 5% | -  | -  | -  | 2% | 3% | 5% |
| Span 20           | 20% | 40%| 50%| 20%| 40%| 50%| -  | -  | -  | -  | -  | -  |
| Cremophor EL-35   | 0.3%| 0.5%| 1% | 0.3%| 0.5%| 1% | -  | -  | -  | -  | -  | -  |
| Ethanol           | 20% | 30%| 45%| 20%| 30%| 45%| 20%| 30%| 45%| 20%| 30%| 45% |
| Distilled water (qs)| 100%| 100%| 100%| 100%| 100%| 100%| 100%| 100%| 100%| 100%| 100%| 100%|
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made gel base at the proportion of 4:1 by slow mixing, followed by manual stirring for 10 min. Disperse Carbopol 934 in distilled water and leave to swell overnight which is used as base for preparation of gel. Propylene glycol is used to dissolve methyl paraben and propyl paraben. The solution is mixed to get the gel mixture. Neutralisation of prepared gel was achieved by adding triethanolamine by frequent stirring until pH (7.0) was obtained and to finally get the consistent translucent gel base.\textsuperscript{19}

Characterization of the tramadol hydrochloride loaded transethosomal gel

Determination of pH

Digital pH meter (Elico LI610) was used to estimate the pH of the gel. A known quantity of transethosomal gel was disseminated in 20ml of distilled water and mixed for 30 min by a mechanical stirrer set to room temperature; the pH of the formulation was read from the digital display.

Viscosity, drug content and EE

Brookfield CAP 2000 viscometer was used to determine the viscosity of tramadol hydrochloride TEs gel using spindle no 16 at 25°C. Drug content was estimated by weighing an amount of transethosomes gel containing tramadol hydrochloride equivalent to 100mg was suspended in suitable media. The final dispersion was kept for 20 min for thorough mixing with often frequent mixing and then it was filtered through 0.45µm membrane filter. The drug content/amount was assessed at 271nm spectrophotometrically using a regression equation of the Beer’s Law plot.\textsuperscript{19}

Stability Studies

Drug EE of transethosomal gel containing 100mg of drug was taken and was dissolved in mixture of DCM (Dichloromethane) and methanol. The dissolved mixture was suspended in 100 ml of phosphate buffer (pH 7.4) and the absorbance was noted at 271nm. From that the amount present in 1ml of transethosomes was obtained. The drug EE was estimated by the formula used in TEs.

The stability studies of tramadol hydrochloride TEs-loaded formulation were performed by keeping freshly made samples of the gel in two sets storage conditions namely at room temperature 25 ± 2°C and refrigerated at 5 ± 3°C and for 28 days.\textsuperscript{15,20} The stored transethosome gel was evaluated for percentage drug content and EE at an interval of 7 days for 28 days.

RESULTS AND DISCUSSION

Transethosomes loaded with tramadol hydrochloride

The tramadol hydrochloride encapsulated transethosomes were formulated for effective pain management by cold method using different lipoidal carrier systems. The cold method was followed for the preparation of TEs as it is very simple and which does not require extreme conditions or sophisticated equipment. Total 12 formulations were developed by using cold method. Formulations were designed using ethanol, edge activator and phospholipid. Span 20 and Cremophor EL-35 were used as edge activators, were as soya lecithin and l-α Phosphatidylethanolamine from egg yolk contributes to lipid carrier and ethanol as solvent system. The size of vesicle is a significant factor that should be consider in the development of Nano carriers for topical drug delivery.\textsuperscript{21} Ethanol is a major component of the ethosomal systems, forgiving exceptional characteristics. 10%–50% is the concentration commonly used. The phospholipid concentration ranged between 0.5 and 5%w/w.\textsuperscript{22} The formulations were developed with the recommended concentration of phospholipid and ethanol.

Drug Excipient compatibility study

Figure 1 epic the FTIR absorption spectrum of pure drug tramadol hydrochloride, which was taken in the range of 700cm\(^{-1}\)--4000cm\(^{-1}\) using KBr disc and the characteristic peak of the drug was observed. The IR spectra of developed formulation and physical mixture and were studied, the results reveals that the characteristic peak of pure drug was predominantly present, which proves the drug and excipients are compatible. No change in shape of spectra observed, indicating that the drug in

![Figure 1: FTIR absorption spectrum of pure drug tramadol hydrochloride.](image-url)
presence of excipients remains stable. The results were shown in Figure 2a and 2b.

**Assay**

The quantity of drug content in the developed transethosome formulation were determined and estimated by UV spectrophotometry at 271 nm. The amount of tramadol hydrochloride in transethosomal formulations was found to be in the range of 91.91 to 95.7%. Among all the formulations F8 was found to be 95.24%. The results of drug content were given in Table 2.

**Percentage drug EE**

The EE of the developed formulations were in the range of 33.43% to 79.43%. The formulations F1 - F3 comprise of Soya lecithin, Span 20 and ethanol as the solvent. Formulation F2 showed higher EE 60.21% and F3 exhibit low EE 33.43%. The effect of variation in entrapment is the presence of ethanol concentration in formulation. Higher concentration of ethanol in the formulation induces the vesicle solubility which leads to leakage of the transethosomal vesicles. The formulation F4 – F6 comprising of L-α phosphatidylcholine from egg yolk, Span 20 and ethanol. Among the formulations F5 showed higher EE63.56% because of optimum concentration ethanol. The formulations F7 – F9 comprising Cremophor EL-35, soya lecithin and ethanol. Formulation F10 – F12 comprising of L-α phosphatidylcholine from egg yolk, Cremophor EL-35 and ethanol as a solvent system. The formulation F7 - F12 was developed with the change in the edge activator Cremophor EL- 35 lead to higher EE. The concentration of the edge activator has a significant role on the transethosome EE. The formulation F8 and F11 showed higher EE78.91% and 79.43% where minimal concentration of ethanol enhances EE. Higher concentration of ethanol in the formulation that induces vesicular solubility which leads to leakage and lower the EE. The results were given in Table 2.

**Evaluation of vesicle size**

The size of vesicles plays an essential role in skin permeation. Smaller vesicular size (< 200 nm) ease the TEs to diffuse by the tiny pores of the skin giving rise to improved permeation. The size was determined by DLS (dynamic light scattering) using a computerized inspection system and photon correlation spectroscopy. The formulation exhibits an average particle size in the range of 149.34 nm to 198.10 nm and the results were shown in Figure 3. The vesicle size of formulations was influenced by the polymer concentration, as the concentration increases the formulations exhibits an increase in vesicle size. Higher concentration of the phospholipids and edge activator produces thick vesicles with high dense and thus increase the size.

<table>
<thead>
<tr>
<th>Formulation Code</th>
<th>Drug content (%) ±SD</th>
<th>EE(%)±SD</th>
<th>Zeta potential ±SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>91.91±0.03</td>
<td>46.45±0.213</td>
<td>-7.76±0.041</td>
</tr>
<tr>
<td>F2</td>
<td>93.97±0.23</td>
<td>60.21±0.034</td>
<td>-9.99±0.053</td>
</tr>
<tr>
<td>F3</td>
<td>94.38±0.041</td>
<td>33.43±0.151</td>
<td>-7.48±0.026</td>
</tr>
<tr>
<td>F4</td>
<td>81.32±0.02</td>
<td>48.37±0.432</td>
<td>-18.59±0.043</td>
</tr>
<tr>
<td>F5</td>
<td>90.99±0.05</td>
<td>63.56±0.031</td>
<td>-21.49±0.043</td>
</tr>
<tr>
<td>F6</td>
<td>92.97±0.04</td>
<td>50.70±0.313</td>
<td>-18.69±0.15</td>
</tr>
<tr>
<td>F7</td>
<td>93.24±0.12</td>
<td>78.91±0.053</td>
<td>-11.53±0.16</td>
</tr>
<tr>
<td>F8</td>
<td>95.39±0.03</td>
<td>78.96±0.041</td>
<td>-19.87±0.091</td>
</tr>
<tr>
<td>F9</td>
<td>89.92±0.41</td>
<td>68.78±0.036</td>
<td>-17.68±0.084</td>
</tr>
<tr>
<td>F10</td>
<td>92.31±0.32</td>
<td>77.37±0.063</td>
<td>-20.61±0.073</td>
</tr>
<tr>
<td>F11</td>
<td>93.56±0.25</td>
<td>79.43±0.121</td>
<td>-22.30±0.082</td>
</tr>
<tr>
<td>F12</td>
<td>95.70±0.13</td>
<td>76.45±0.0143</td>
<td>-18.30±0.043</td>
</tr>
</tbody>
</table>
The size of the vesicles was further influenced by the type of phospholipid used in the development of formulation. The vesicle size was increased due to increased fusion of lipid bilayer and consequent increase in surface free energy that ultimately occur by the influence of density of lipids. Formulation developed using soya lecithin exhibits an increased particle size than egg yolk formulations. Soya lecithin formulations are viscous than the 1-α Phosphatidylcholine from egg yolk formulations.

The presence of the edge activator plays significant role in vesicular size. Formulation using Span 20 exhibits lager vesicular size than Cremophor EL-35. As the concentration of edge activator increases, the formulation exhibits a decrease in vesicular size.

**Transethosomes Morphology**

The morphology of the TE formulations was visualized by the TEM. The TE formulations had asymmetrical shape. This might be ascribed to the presence of the edge activator (Cremophor EL-35 and Span 20) in the composition of the vesicles which flustered the lipid bilayer and raised their fluidity. The TEM of tramadol loaded transethosomes was shown in Figure 4 and 5.

**Zeta potential**

The zeta potential analysis was performed to investigate the surface charge properties of TE formulations. The transethosome stability and interaction of formulation with skin was influenced by zeta potential. Presence of ethanol in formulation exhibits a negative charge on the polar groups of phospholipids that build an electrostatic repulsion. The zeta potential of the transethosomes was found between the ranges of -7.76 mV to -22.30 mV. The zeta potential peak of charge -22 mV was shown in Figure 6. Thus, it was concluded that the TE system had sufficient stability. The results were given in Table 2.

**In vitro drug release**

The in vitro diffusion studies were performed for the prepared TE formulations by using Franz diffusion cell. The results of diffusion studies conducted for TE formulations containing tramadol hydrochloride were reported in Figure 7a and 7b.

**Effect of Edge Activator**

![Figure 3: Vesicle Size of Transehosome Formulations F1 - F12.](image)

![Figure 4: TEM of the Transehosome Formulation Containing Edge Activator Cremophor EL-35.](image)

![Figure 5: TEM of the Transehosome Formulation Containing Edge Activator Span 20.](image)

![Figure 6: Zeta Potential of optimised transehosome formulation.](image)
The use of edge activator in formulation increases the skin permeability and there which increases the release of tramadol. The in vitro release of transethosomes prepared by Span 20 as edge activator exhibits a higher rate of release than Cremophor EL-35. Cremophor EL-35 formulations exhibits controlled release over span, the tendency is due to viscous nature of edge activator. Formulation F1-F6 prepared with span exhibit a drug release of 90.12% to 94.99% which is higher than cremophor formulations (F7– F12, 88.34% to 82.19%) at the end of 8th hr.

**Effect of Ethanol**

The formulations were developed using increase concentration of ethanol as permeation enhancer. Ethanol is an efficient penetration enhancer; the concentration of ethanol influences the solubility of lipids. As the concentration of ethanol increases, lipid vesicle miscibility increases. Among the developed formulations, those prepared with 40% exhibits a rapid release than the other at the end of 8th hr. Formulation F8 and F11 prepared with 30% of ethanol as solvent exhibits a controlled drug release of 78.96% and 79.98% at the end of 8th h. An optimized concentration proves to be controlled.

**Effect of Phospholipid**

The phospholipid bilayer in vesicular formulation can influence both encapsulation and release of the drug particles. The nonpolar hydrophobic part of the phospholipid has more affinity towards the skin thus fuses with the lipid content of the skin and facilitates the delivery of the entrapped material. The formulation was developed by using soya lecithin and egg yolk as phospholipid. The phospholipid was used at a concentration of 2%, 3% and 5%. Formulation developed with higher concentration of phospholipid exhibits a faster release than with the lower concentration with 3% due to greater affinity towards the skin.

Among all formulations, F11 comprising ethanol 30% and 2% of phospholipid and suitable edge activator (Cremophor EL-35) has found to be the optimum batch which exhibits a controlled release of tramadol hydrochloride from the TEs formulation at the end of 8th hr. Further the formulation F11 is considered for the development of transethosomal gel formulation.

**Analysis of release mechanism**

The release data of tramadol hydrochloride transethosome formulation F11 was fitted into various kinetic models such as zero order, first order and highchair in order to analyse the mechanism of release of tramadol hydrochloride from TEs. The release pattern of the formulation F11 exhibit best fit of highest correlation coefficient in First order kinetics R² value 0.991. Hence the formulation follows diffusion followed by dissolution pattern.

**Characterization of the tramadol hydrochloride loaded transethosomal gel**

The cold method was followed for the making of tramadol hydrochloride transethosomes. Among the prepared formulations the optimised batch was incorporated into carbopol 934 gel base. The prepared tramadol hydrochloride gel was further characterised for pH, viscosity, drug content and EE. The results of characterization of the tramadol hydrochloride-loaded transethosomal gels are briefed in Table 3. The pH of the preparation was found to be 7.0; the transethosome gel formulation was evaluated for viscosity, drug content and EE. The viscosity of the transethosomal gel formulation was found to be 30168 cps, the drug content and EE of transethosomal gel was found to be 91.52 and 79.37% respectively.
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Table 3: Characterisation of TEs gel formulation.

<table>
<thead>
<tr>
<th>Formulation</th>
<th>pH</th>
<th>Viscosity</th>
<th>Drug Content</th>
<th>EE</th>
</tr>
</thead>
<tbody>
<tr>
<td>Transethosomal gel formulation</td>
<td>7.0</td>
<td>30168cps</td>
<td>91.52%</td>
<td>79.37%</td>
</tr>
</tbody>
</table>

Stability Studies

The refrigerated condition (5±3°C) and (25±2°C) for 28 days was used to study the stability of developed gel formulation. The Transethosomal gel was evaluated for drug content and EE at an interval of 7 days for 28 days. A negligible loss of drug is seen in refrigerated condition and room temperature. There is very less change in the EE, which proves that the formulation was found to be stable. The results of the stability studies of the gel in both the temperature conditions are summarized in Figure 8 and 9.

CONCLUSION

Tramadol hydrochloride is a opiate analgesic acts as a µ-opioidreceptor. The tramadol hydrochloride encapsulated transethosomes were formulated for effective pain management by cold method with different lipoidal carrier systems. Total 12 formulations were prepared by using cold method. Formulations were designed using ethanol, edge activator and phospholipid. Span 20 and Cremophor EL-35 were used as edge activators, soya lecithin and l-α Phosphatidylecholine from egg yolk contributes to lipid carrier and ethanol as solvent system. The physical evaluation of pure drug and along with excipients has shown compatibility. The FTIR results reveal that there is no interaction between the drug and excipient of the formulations. The drug content of the transethosomal formulations was fit to be in the range of 91.91 to 95.7% and formulations F8 and F11 showed higher EE78.96% and 79.34% than other batches. The formulation exhibits an average particle size in the range of 149.34nm to 198.10nm. As the concentration of edge activator increases in the formulation shows decrease vesicular size. Formulation developed using soya lecithin exhibits an increased particle size than egg yolk formulations. Soya lecithin formulations are viscous than the l-α Phosphatidylecholine from egg yolk formulations. The zeta potential of the transethosomal formulations was found between the ranges of -7.76 mV to -22.69 mV. The optimized formulation F11 shows -22 mV and proven to be sufficient stable. Formulation F11 comprises an optimum concentration of ethanol 30% with optimum concentration of phospholipid 3% with a suitable edge activator (Cremophor EL-35) has found to be the optimum batch which exhibits a controlled rate of release of tramadol hydrochloride of 79.98% at the 8th hr. The release pattern of the formulation F11 exhibit best fit of highest correlation coefficient by the First order kinetics. The gel formulation was studied for viscosity, drug content and EE. The gel characteristics were found to be satisfactory. The stability studies given away that the formulation was stable at refrigerated conditions (5 ± 3°C) for 28 days. Therefore, the study proves that transethosomal gel is possible carrier for the topical delivery of tramadol hydrochloride. These afford another route for the administration of the drug to conquer the reduced bioavailability and rigorous side effects connected with the oral route.

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CONFLICT OF INTEREST

The authors declare no conflict of interest.
ABBREVIATIONS

**TEs:** Transethosomes; **TEM:** Transmission electron microscopy; **Rpm:** Revolutions per minute; **°C:** Degree Celsius; **mg:** Milligram; **FTIR:** Fourier transform infrared spectroscopy; **EE:** Entrapment efficiency.

REFERENCES


SUMMARY

- The tramadol hydrochloride encapsulated transethosomes were formulated for effective pain management by cold method using different lipoidal carrier systems. Tramadol hydrochloride is a centrally acting opiate analgesic. Topically applied opioid predominately have central effects which plays a primary role on peripheral nervous system. The developed transethosomes were characterized for FTIR, drug content, EE, particle size, zeta potential, TEM, in vitro drug release and release kinetics.
- The in vitro release of the transethosomes was extensively studied and the effect of the edge activator, ethanol and phospholipid concentration on release studies was estimated by using Franz diffusion cell. From in vitro studies it was concluded that the release of tramadol hydrochloride was influenced by changing the ratio of phospholipid and ethanol. The optimised formulation was considered for topical gel preparation.
PICTORIAL ABSTRACT

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